

# Cardiac responses to auditory irregularities reveal hierarchical information processing during sleep

Matthieu Koroma<sup>1,2</sup>, Paradeisios Alexandros Boulakis<sup>1,2</sup>, Federico Raimondo<sup>3,4</sup>, Vaia Gialama<sup>1,2</sup>, Christine Blume<sup>5,6,7</sup>, Mélanie Strauss<sup>8,9</sup> and Athena Demertzi<sup>1,2</sup>

1 CRC Human Imaging Unit, GIGA Institute, Allée du 6 Août, 8 (B30), 4000 Sart Tilman, University of Liège, Liège, Belgium

2 Department of Psychology, Psychology and Neuroscience of Cognition Research Unit, University of Liège, Liège, Belgium

3 Institute of Neuroscience and Medicine, Brain and Behaviour (INM-7), Research Center Jülich, Jülich, Germany

4 Institute of Systems Neuroscience, Medical Faculty, Heinrich Heine University Düsseldorf, Düsseldorf, Germany

5 Centre for Chronobiology, Psychiatric Hospital of the University of Basel, Basel, Switzerland

6 Research Cluster Molecular and Cognitive Neurosciences, University of Basel, Basel, Switzerland

7 Department of Biomedicine, University of Basel, Switzerland

8 Université libre de Bruxelles (ULB), Hôpital Universitaire de Bruxelles (H.U.B), CUB Hôpital Érasme, Service de Neurologie et Unité Fonctionnelle Sommeil et Vigilance, Route de Lennik 808, 1070 Brussels, Belgium

9 Laboratory of Experimental Neurology, ULB Neuroscience Institute, Université Libre de Bruxelles, Brussels, Belgium

**Keywords:** brain-heart interactions, ECG, local-global paradigm, sleep, auditory processing

## Abstract

Our ability to process environmental stimuli varies during sleep. Although much research focused on neural processing, emerging evidence shows that bodily signals may play a key role in understanding high-level sensory processing during sleep. Here, we tested how cardiac responses to the local-global paradigm, a typical oddball task probing the processing of simple (local) and complex (global) sensory irregularities. To do so, we analyzed electrocardiography (ECG) signals in a total of 56 participants from two existing datasets which contained cerebral responses to local auditory irregularities, but which did not analyze the ECG data before. We found that cardiac activity slowed down after global, but not local, auditory irregularities, revealing the presence of global deviance effect in Rapid Eye Movement (REM) sleep. In contrast, cardiac activity was faster after local, but not global, deviants in Non-Rapid Eye Movement (NREM) sleep. Overall, our results demonstrate that cardiac responses to auditory irregularities inform about hierarchical information processing and its variations during sleep beyond cerebral activity. They highlight the embodiment of cognitive function and the value of cardiac signals to understand the variations of sensory processing during sleep.

## Introduction

Sleep is classically considered as a state of loss of vigilance to the external world (Peigneux et al., 2001). Yet, remaining sensitive to the environment during sleep might be crucial for survival, allowing, for example, to wake up if unexpected events occur (Blume & Schabus, 2019; Cirelli & Tononi, 2008; Coenen, 2024). Previous investigations on the neural responses to sounds of different complexities have revealed that the sleeping brain indeed processes from simple acoustic stimuli up to semantic information, but that this ability depends greatly on sleep states (Andrillon & Kouider, 2020; Hennevin et al., 2007).

In comparison, how the body is involved in complex auditory information processing during sleep has been so far understudied (Koroma et al., 2024). Yet, emerging evidence suggests that bodily signals play also a fundamental role in cognition and perception (Azzalini et al., 2019). Empirical support highlighting the importance of bodily signals has been obtained by showing for example that cardiac activity responses to sound inform about the classification of disorders of consciousness beyond neural activity in the local-global paradigm (Raimondo et al., 2017).

The local-global paradigm is a classical mismatch detection task probing loss of vigilance to hierarchical information by distinguishing between an automatic detection of low-level auditory irregularities (local mismatch effect), and a consciousness-dependent detection of high-level auditory irregularities (global deviance effect) (Bayne et al., 2024; Bekinschtein et al., 2009). By applying this paradigm to sleep, neural signatures of local mismatch detection, but not of global deviance detection, have been previously reported (Blume et al., 2022; Strauss et al., 2015, 2022). However, the investigation of the cardiac correlates of hierarchical information processing during sleep remained to be performed.

In the present study, we tested how cardiac responses were shaped by auditory irregularities of different complexities during healthy sleep. In line with brain results, we hypothesized that

local mismatch and global deviance effects would be observed at the cardiac level during wakefulness (Blume et al., 2022; Strauss et al., 2015, 2022). In comparison, only local mismatch effects would be found during sleep, reflecting the breakdown of hierarchical information processing (Blume et al., 2022; Makov et al., 2017; Strauss et al., 2015).

As a secondary hypothesis, we predicted that cardiac effects would depend on sleep states. In particular, cardiac responses would be preserved in light NREM (*i.e.*, NREM2) and periods of REM sleep without eye movements (*i.e.*, tonic REM), during which a wide range of sensory processing (*e.g.*, preferentially reacting to one's own name) is preserved (Andrillon & Kouider, 2020; Perrin, 1999). In contrast, cardiac responses would be absent in deep NREM (*i.e.*, NREM3) and periods of REM sleep without eye movements (*i.e.*, phasic REM), during which auditory information is typically suppressed (Ermis et al., 2010; Koroma et al., 2020; Legendre et al., 2019).

## Methods

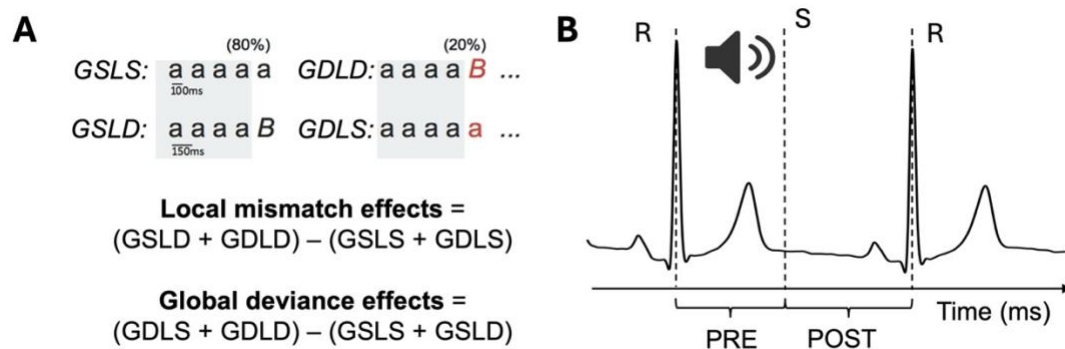
### *Local-global paradigm during sleep*

We extracted the electrocardiographical (ECG) signals of 56 healthy young adults from 18 to 35 years old who heard the local-global paradigm during wakefulness and sleep ( $n=28$  for a morning nap from Strauss et al., 2015;  $n=28$  for 2 full nights from Blume et al., 2022). Stimuli were pairs of phonetically distant vowels (100 ms duration). Five vowels with a 50 ms interstimulus interval were included in each trial. The first four vowels were identical, and the last one was either the same ("local standard") or different ("local deviant"; cf. Figure 1A, top).

Trials were presented in two types of blocks and the vowels serving as standards and deviants were counterbalanced across repetitions of blocks. In one block, 80% of the sequences were composed of five identical sounds (aaaaa), referred to as "Global Standard Local Standard" (GSLS), and 20% of four identical sounds and a deviant (aaaaB), referred to as

“Global Deviant Local Deviant” (GDLD). The proportions were reversed in another block with composing 80% of the sequences composed of four identical sounds and a deviant (aaaaB), referred as “Global Standard Local Deviant” (GSLD), and 20% of five identical sounds (aaaaa), referred as “Global Deviant Local Standard” (GDLS; Figure 1A, top).

Using the same methodology as adopted for cerebral signals (Bekinschtein et al., 2009; Blume et al., 2022; Strauss et al., 2015), the local mismatch effect was defined by subtracting local deviants from the local standards: (GSLD+GDLD) - (GSLS+GDLS); and the global deviance effect by subtracting global deviants from global standards: (GDLS+GDLD) - (GSLS+GDLD) (Figure 1A, bottom). To control for potential confounding effects between local mismatch and global deviance effects, we further checked the contrast between local deviants and local standards using global standard trials only, defining the ‘true local’ effect as: (GSLD - GSLS). We also controlled the contrast between global deviant and global standards using local standard trials only, defining the ‘true global’ effect as: (GDLS - GSLS).



**Figure 1. Analysis of the local-global paradigm played during sleep across two datasets.**

**(A)** A trial was composed of a sequence of 5 tones and belonged to one of the 4 following categories: global standard and local standard (GSLS, top left), global deviant and local deviant (GDLD, top right), global standard and local deviant (GSLD, bottom left), global deviant and local standard (GDLS, bottom right). The combination of responses to these trials allows to define local mismatch and global deviance effects. Adapted from (Strauss et al., 2022)

**(B)** Heartbeat was extracted from ECG and the duration between onset of the 5th sound and the preceding (PRE) and following heartbeat (POST) was computed for each trial following the methodology of (Raimondo et al., 2017).

### *Cardiac analyses during wakefulness and sleep*

Heartbeats were extracted after cleaning the ECG signal (sampled at 120 Hz) using the *ecg\_process* function (high-pass Butterworth filter at 0.5 Hz and powerline filter at 50 Hz) and identifying R-peaks with the *neurokit* method from the Neurokit2 package (Makowski et al., 2021). For assessing variations of baseline cardiac activity, interbeat intervals (RR) were computed as a proxy for heart rate during wakefulness and sleep. The values were averaged for wakefulness and each sleep stages within each participant.

Following previous methodology (Raimondo et al., 2017), the cardiac responses to local mismatch and global deviance were obtained by comparing the modulation of the heartbeat timing before and after the occurrence of low-level and high-level auditory irregularities during wakefulness and sleep. The interval between the onset of the fifth sound of each trial with the preceding and following heartbeats defining respectively a PRE and a POST period for each trial (Figure 1C). Sufficient signal-to-noise ratio was ensured by keeping for further analyses sleep stages within each participant that counted at least 10 deviant trials.

As in Raimondo and colleagues (2017), our analyses were first restricted to trials for which both PRE and POST intervals were contained between 20 and 600 ms around the fifth sound onset. Using a grid-search procedure, we also extended analyses by testing for local mismatch and global deviance effects on time-windows between 20 and 600 ms up until 20 and 1200ms with 100ms step interval. To do so, values were first averaged within each participant and compared between PRE and POST periods for wakefulness and sleep.

### *Comparisons of cardiac modulation during wakefulness and sleep*

Sleep scoring was performed offline according to the AASM guidelines (Iber et al., 2007) as reported in associated publications (Blume et al., 2022; Strauss et al., 2015). Eye movements in REM sleep were identified by independent scorers (M.S. for the Strauss dataset; M.K. and

V.G. for the Blume dataset), defining trials with eye movements as phasic REM, and without eye movements as tonic REM (Simor et al., 2020). NREM1 was excluded from analyses as it is considered a transitional sleep stage (Lacaux et al., 2024; Ogilvie, 2001).

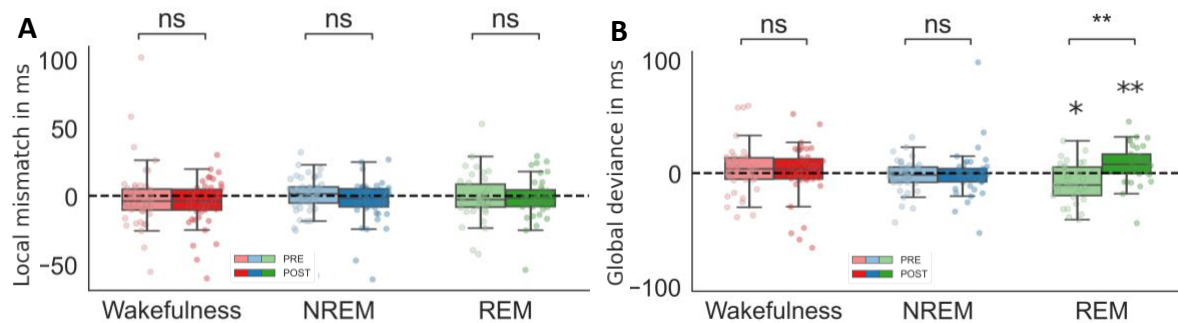
The modulation of heart rate and local mismatch and global deviance effects for PRE and POST periods across sleep stages were tested with linear mixed models with participants as random factor using the *lmer* package in R. Post-hoc comparisons were tested with non-parametric Wilcoxon and Mann-Whitney tests using the *scipy* toolbox and absence of effects with Bayes Factors analyses using the *Pinguoin* toolbox in Python. Multiple comparisons were corrected using false detection rate (alpha threshold=0.05) (Benjamini & Yekutieli, 2001).

Median and 95% confidence interval (95CI) of beta estimates ( $\beta$ ), standardized  $\beta$  and  $t$  values ( $t$ ) are reported for mixed-model analyses. Median and 95CI (bootstrap,  $n=2000$ ) and effect sizes, according to the formula  $r = z/\sqrt{n}$ ,  $z$  being the  $z$ -stats of the Wilcoxon signed rank test and  $n$  being the number of participants, were reported for non-parametric post-hoc tests. Bayes Factors (BF) were reported with values above 3 being considered as positive evidence in favor of the null hypothesis (Kass & Raftery, 1995).

## Results

### *Cardiac activity slows down after global deviants in REM sleep.*

In terms of the local mismatch effect, there was no evidence for a cardiac modulation (PRE vs. POST:  $\beta=4.11\pm[-3.0, 11.23]$ ,  $t(256)=1.14$ ,  $p=0.26$ , standardized  $\beta=0.24\pm[-0.17, 0.64]$ ). The effect was not evidenced across vigilance stages (POST vs. PRE with: Wakefulness vs. NREM:  $\beta=0.43\pm[-9.63, 10.49]$ ,  $t(256)=0.08$ ,  $p=0.93$ , standardized  $\beta=0.02\pm[-0.55, 0.60]$ ; Wakefulness vs. REM:  $\beta=3.47\pm[-7.18, 14.11]$ ,  $t(256)=0.64$ ,  $p=0.52$ , standardized  $\beta=0.20\pm[-0.41, 0.81]$ ). Post-hoc testing confirmed the absence of the local mismatch effect in both wakefulness, NREM and REM sleep (all tests:  $p>0.05$ ,  $BF>3.0$ ) (Figure 2A).



**Figure 2. Cardiac activity decelerates after global deviants in REM sleep.** Local mismatch (**A**) and global deviance (**B**) effects of cardiac responses were computed for Wakefulness, NREM and REM separately for the PRE and POST periods with respect to the fifth sound of the local-global paradigm (contained between 20 and 600ms). Boxplots represent median, 1<sup>st</sup> and 4<sup>th</sup> quartiles and deciles of effects across subjects are represented by boxplots in each sleep state. Datapoints represent individual subjects. Statistical significance of post-hoc tests, ns: not significant, \*:  $p < 0.05$ , \*\*:  $p < 0.01$ .

In terms of the global deviance effect, there was a difference between Wakefulness and REM sleep (POST vs. PRE and Wakefulness vs. REM:  $\beta = 19.91 \pm [6.52, 33.29]$ ,  $t(224) = 2.93$ ;  $p = 0.004$ , standardized  $\beta = 0.95 \pm [0.31, 1.58]$ ; POST vs. PRE and NREM vs. REM:  $\beta = 13.07 \pm [-0.38, 26.53]$ ,  $t(224) = 1.91$ ,  $p = 0.06$ , standardized  $\beta = 0.62 \pm [0.31, 1.58]$ ). Post-hoc tests uncovered a cardiac deceleration after global deviants in REM (POST vs. PRE:  $r = -0.52$ ,  $p = 0.002$ ; PRE:  $-9.37 \pm [-11.95, 1.38]$ ,  $r = -0.39$ ,  $p = 0.02$ ; POST:  $8.76 \pm [4.51, 13.72]$ ,  $r = 0.54$ ,  $p = 0.004$ ). Such modulation was absent in Wakefulness and NREM (Wakefulness: POST vs. PRE:  $r = -0.03$ ,  $p = 0.84$ ,  $BF = 5.38$ ; PRE:  $4.72 \pm [-0.16, 9.30]$ ,  $r = -0.14$ ,  $p = 0.84$ ,  $BF = 2.2$ ; POST:  $4.75 \pm [-2.84, 7.50]$ ,  $r = -0.00$ ,  $p = 0.84$ ,  $BF = 5.3$ ; NREM: POST vs. PRE:  $-0.56 \pm [-5.18, 4.38]$ ,  $r = -0.03$ ,  $p = 0.85$ ,  $BF = 5.0$ ; PRE:  $r = -0.11$ ,  $p = 0.84$ ,  $BF = 3.7$ ; POST:  $0.00 \pm [-3.54, 2.48]$ ,  $r = -0.07$ ,  $p = 0.84$ ,  $BF = 5.9$ ) (Figure 2B).

We also tested for the presence of the “true local” effects by restricting analyses on global standard trials only (GSLD - GSLS) and “true global” effects by restricting analyses on local standard (GDLS - GSLS). The linear mixed-effects model showed the presence of a “true global” deviance effect in REM sleep as compared to wakefulness ( $\beta = 27.9 \pm [10.16, 45.60]$ ,

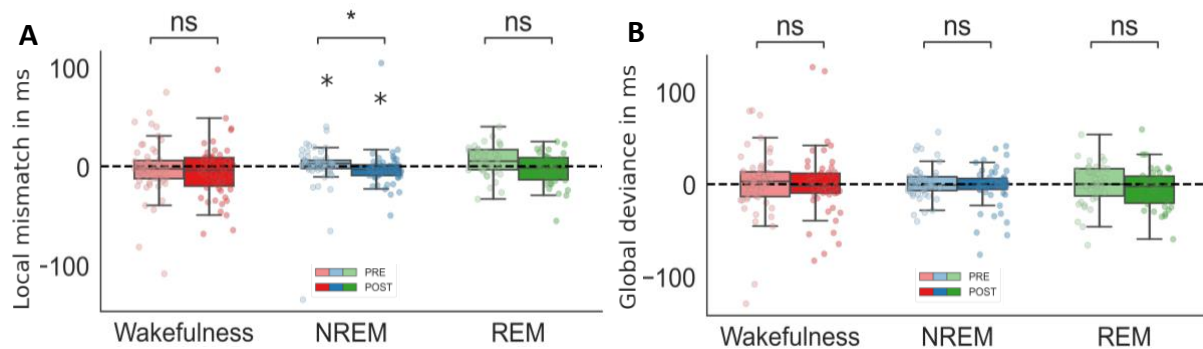


$t(182)=3.10$ ,  $p=0.002$ , standardized  $\beta=1.11\pm[0.40, 1.81]$ ), and post-hoc tests confirmed that this was due to a cardiac deceleration after global deviants in REM sleep (POST vs. PRE:  $r=0.50$ ,  $p=0.009$ ; PRE:  $-11.51\pm[-14.01, 0.71]$ ,  $r=-0.30$ ,  $p=0.12$ ; POST:  $-11.92\pm[3.58, 23.37]$ ,  $r=0.44$ ,  $p=0.043$ , Figure S3B). The modulation of cardiac responses was absent for the true local mismatch effects in wakefulness and sleep (all tests:  $p>0.05$ ,  $BF>3.0$ , Figure S3A).

*Cardiac activity accelerates after local deviants in NREM sleep.*

As NREM was characterized by lower heart rate than Wakefulness ( $\beta=70.43\pm[20.10, 120.76]$ ,  $t(141)=2.77$ ,  $p=0.006$ , Standardized  $\beta=0.46\pm[0.13, 0.63]$ ; NREM vs. Wakefulness,  $r=0.33$ ,  $p=0.017$ ; Figure S1A), we investigated local mismatch and global deviance effects beyond the restriction of analyses on PRE and POST periods between 20 to 600ms based on Raimondo and colleagues (Raimondo et al., 2017) (Figure S2). A grid search analysis revealed the presence of a local mismatch effect between 20 and 900ms during sleep (PRE vs. POST:  $p=0.045$ , corrected Wilcoxon test). No other effects were evidenced neither in sleep nor wakefulness ( $p>0.05$  for all tests) (Table S1).

Post-hoc comparisons showed that cardiac activity accelerated after local deviants in NREM sleep (POST vs. PRE:  $r=-0.33$ ,  $p=0.017$ ; PRE:  $3.92\pm[1.36, 5.16]$ ,  $r=-0.35$ ,  $p=0.02$ ; POST:  $-2.27\pm[-4.39, -0.35]$ ,  $r=-0.27$ ,  $p=0.046$ ). We also confirmed an absence of modulation of cardiac activity after local deviants in Wakefulness and REM sleep (Wakefulness: POST vs. PRE:  $r=-0.29$ ,  $p=0.61$ ,  $BF=6.3$ ; PRE:  $-1.67\pm[-5.79, 2.61]$ ,  $r=-0.06$ ,  $p=0.64$ ,  $BF=6.5$ ; POST:  $-2.74\pm[-10.39, 6.02]$ ,  $r=-0.16$ ,  $p=0.46$ ,  $BF=4.1$ ; REM: POST vs. PRE:  $r=-0.29$ ,  $p=0.07$ ,  $BF=1.3$ ; PRE:  $6.15\pm[0.65, 13.66]$ ,  $r=0.41$ ,  $p=0.03$ ,  $BF=0.32$ ; POST:  $-0.83\pm[-5.13, 4.04]$ ,  $r=-0.08$ ,  $p=0.62$ ,  $BF=4.3$ ). (Figure 3A). As expected from the grid search analysis, global deviance effects were also absent in wakefulness and sleep ( $p>0.05$  and  $BF>3.0$  for all tests) (Figure 3B).

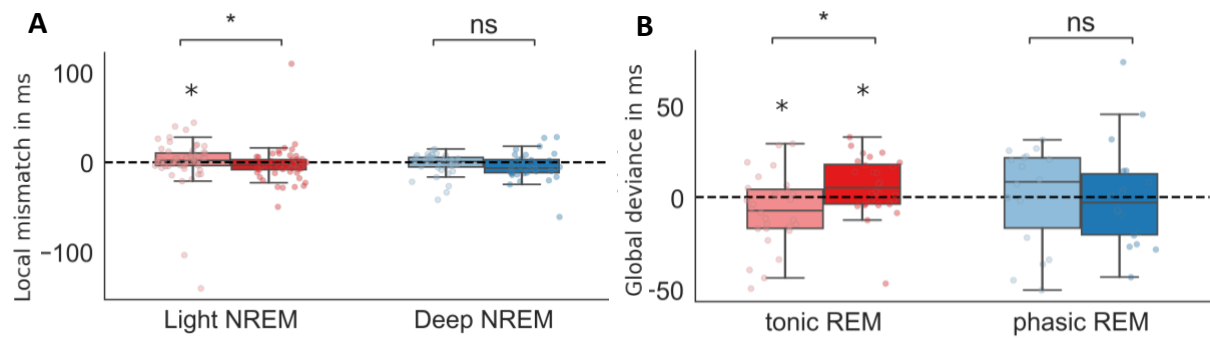


**Figure 3. Cardiac activity accelerates after local deviants during NREM sleep.** Local mismatch (A) and global deviance (B) effects were computed for Wakefulness, NREM and REM separately for PRE and POST periods (contained between 20 and 900ms, following a grid-search analysis). Boxplots represent median, first and fourth quartiles and whiskers deciles for each condition. Datapoints represent individual subjects. Statistical significance for post-hoc test, ns: not significant, \*:  $p < 0.05$

We further checked whether “true local” effects were also observed in NREM sleep. Post-hoc effects showed that cardiac activity was modulated around local deviants after restricting our analyses on global standard trials only during NREM sleep (POST vs. PRE:  $r = -0.33$ ,  $p = 0.016$ ; PRE:  $3.77 \pm [-1.09, 5.64]$ ,  $r = -0.25$ ,  $p = 0.07$ ; POST:  $-2.76 \pm [-5.00, 1.37]$ ,  $r = -0.26$ ,  $p = 0.07$ ) (Figure S4A). We also confirmed that “true global” deviance effects were not observed in wakefulness nor sleep (all tests:  $p > 0.05$ ,  $BF > 3.0$ , Figure S4B).

#### *Cardiac activity is modulated by auditory deviants in light NREM and tonic REM sleep.*

As local mismatch effects were evidenced during NREM sleep and global deviance effects during REM sleep, we tested our secondary hypotheses. We predicted that cardiac effects were observed in light NREM and periods of REM sleep without eye movements, referred to as tonic REM, during which auditory information is processed (Andrillon & Kouider, 2020; Ermis et al., 2010; Rechtschaffen et al., 1966). In line with the literature (Arnulf, 2011; Spreng et al., 1968), our scoring resulted in identifying  $20 \pm 12\%$  (mean  $\pm$  standard deviation) trials with elevated eye-movement activity during REM sleep, referred as phasic REM (Figure S1B).



**Figure 4. Cardiac responses were modulated in light NREM and tonic REM sleep.** Local mismatch effects were computed for PRE and POST periods contained between 20 and 900ms in light and deep NREM (A) and between 20 and 600ms global deviance effects in tonic and phasic REM (B). Boxplots represent median, first and fourth quartiles and whiskers deciles for each condition. Datapoints represent individual subjects. Statistical significance for post-hoc test, ns: not significant, \*:  $p < 0.05$

Using preprocessing time-windows between 20 and 900 ms, post-hoc tests confirmed the presence of local mismatch effects in light NREM (POST vs. PRE:  $r = -0.27$ ,  $p = 0.04$ ; PRE:  $2.94 \pm [-1.22, 5.60]$ ,  $r = 0.31$ ,  $p = 0.05$ ; POST:  $-2.56 \pm [-4.23, 0.47]$ ,  $r = -0.22$ ,  $p = 0.10$ ). Effects were not significant in deep NREM (POST vs. PRE:  $r = -0.24$ ,  $p = 0.16$ ,  $BF = 4.3$ ; PRE:  $1.73 \pm [-2.08, 5.34]$ ,  $r = 0.08$ ,  $p = 0.65$ ,  $BF = 4.7$ ; POST:  $-5.43 \pm [-9.15, 1.37]$ ,  $r = -0.28$ ,  $p = 0.18$ ,  $BF = 2.0$ ) (Figure 4A). Using preprocessing time-windows between 20 and 600 ms, post-hoc tests confirmed the presence of a cardiac deceleration after global deviants in tonic REM and its absence in phasic REM (tonic REM: POST vs. PRE:  $r = 0.19$ ,  $p = 0.02$ ; PRE:  $r = -0.12$ ,  $p = 0.12$ ; POST:  $r = 0.23$ ,  $p = 0.03$ ; phasic REM: POST vs. PRE:  $r = 0.08$ ,  $p = 0.77$ ,  $BF = 4.1$ ; PRE:  $9.29 \pm [-10.18, 22.05]$ ,  $r = 0.01$ ,  $p = 0.83$ ,  $BF = 4.0$ ; POST:  $-2.01 \pm [-18.37, 12.12]$ ,  $r = -0.10$ ,  $p = 0.83$ ,  $BF = 4.1$ ) (Figure 4B).

“True local” mismatch effects failed to reach significant levels in light NREM sleep and deep NREM sleep (light NREM: POST vs. PRE:  $r = -0.21$ ,  $p = 0.09$ ,  $BF = 5.8$ ; PRE:  $2.93 \pm [0.39, 5.43]$ ,  $r = 0.22$ ,  $p = 0.22$ ,  $BF = 4.8$ ; POST:  $-0.71 \pm [-4.48, 2.00]$ ,  $r = -0.11$ ,  $p = 0.41$ ,  $BF = 6.6$ ; deep NREM: POST vs. PRE:  $r = -0.14$ ,  $p = 0.41$ ,  $BF = 5.6$ ; PRE:  $-0.01 \pm [-3.50, 5.31]$ ,  $r = 0.05$ ,  $p = 0.77$ ,  $BF = 2.32$ ; POST:  $-4.60 \pm [-8.47, -2.65]$ ,  $r = -0.33$ ,  $p = 0.10$ ,  $BF = 1.91$ ) (Figure S4A). “True global” deviance effects were confirmed in tonic REM with a stronger cardiac deceleration after global

deviants in local standard trials (POST vs. PRE:  $r=-0.18$ ,  $p=0.27$ ,  $BF=0.6$ ; PRE:  $-9.65\pm[-15.68, 4.73]$ ,  $r=-0.12$ ,  $p=0.37$ ,  $BF=3.4$ ; POST:  $9.18\pm[0.78, 20.59]$ ,  $r=0.15$ ,  $p=0.04$ ) (Figure S4B). This effect was not observed during phasic REM (POST vs. PRE:  $r=0.18$ ,  $p=0.56$ ,  $BF=2.1$ ; PRE:  $-28.42\pm[-52.78, 16.75]$ ,  $r=-0.21$ ,  $p=0.31$ ,  $BF=1.3$ ; POST:  $-1.91\pm[-36.83, 29.51]$ ,  $r=-0.04$ ,  $p=1.0$ ,  $BF=2.6$ ) (Figure S4B).

## Discussion

We investigated the modulation of cardiac activity by hierarchical auditory irregularities presented during wakefulness and sleep. We report that cardiac activity slows down after complex auditory irregularities (global deviance effect) in REM sleep, and that it accelerates after basic irregularities (local mismatch effect) in NREM sleep. These results open a discussion not only about the contribution of bodily signals in understanding cognitive processing, but also about the variations of sensory processing depending on sleep stages and their associated markers, such as rapid eye movements and slow-wave activity.

In contrast to cerebral findings, we showed an absence of local mismatch and global deviance effects at the cardiac level during wakefulness. This absence of an effect can be explained by the inhibition of cardiac modulations by the prefrontal cortex, a region active during wakefulness and deactivated during sleep (Muzur et al., 2002; Wong et al., 2007). These findings also replicate previous observations that cardiac activity is not modulated by the local and global auditory irregularities in healthy awake controls (Raimondo et al., 2017).

Contrary to our hypothesis, we further found that cardiac activity slows down after global deviants during REM sleep. The detection of global deviance in REM sleep might indicate the preservation of a form of error-related monitoring that has been typically associated with the slowdown of cardiac activity (see Skora et al., 2022 for a review). The restriction of global deviance effects to tonic REM sleep is in line with the fact that the processing of auditory

stimuli is suppressed in presence of rapid eye movements during REM sleep (Ermis et al., 2010; Koroma et al., 2020; Sallinen et al., 1996; Wehrle et al., 2007).

In line with our hypothesis, we observed that cardiac activity was faster after local deviants in NREM sleep. These findings confirm previous observations that auditory mismatch triggers an acceleration of cardiac activity accompanied with a transient increase of arousal in NREM sleep (de Zambotti et al., 2018). They also confirm that the detection of local mismatch is preserved during NREM sleep, as previously observed in cerebral responses to local deviants (Blume et al., 2022; Strauss et al., 2015).

The variations of cardiac responses to auditory irregularities of different complexities can be interpreted in the light of variations of brain-heart interactions during sleep (Chouchou & Desseilles, 2014). Global effects found in REM and local effects in NREM can showcase the different levels of cardiac control between higher-level cortical areas involved in complex interoceptive and sensory information processing (*e.g.*, insula) in REM sleep (Bamiou et al., 2003; Oppenheimer & Cechetto, 2016) and lower-level brain regions associated with automatic arousal reactions (*e.g.*, brainstem) in NREM sleep (Benarroch, 2018; Griffiths et al., 2001). The cardiac slowdown observed in REM and acceleration in NREM may further reflect the release from a cardiac control by the predominant sympathetic activity in REM sleep (Postuma et al., 2010) and parasympathetic tone in NREM sleep (Vigo et al., 2010; Viola et al., 2011).

Our results on cardiac responses during sleep can be further compared with those obtained in patients with disorders of consciousness (DOC) (Raimondo et al., 2017). In that study, cardiac responses to global deviance effects were found in patients who exhibit complex behaviors and cognitive processing in minimally conscious state as compared to unresponsive wakefulness syndrome (Laureys, 2005), which aligns with our findings considering that more complex cognitive activities are typically observed during REM sleep as compared to NREM sleep (Tononi et al., 2024; Tononi & Massimini, 2008). Noteworthy, global deviance effects

manifested as a slowdown of cardiac activity in REM sleep and as a cardiac acceleration in DOC patients in minimally conscious states, further highlighting the differences in autonomic regulation between sleep and DOC states (Raimondo et al., 2017).

Overall, our results extend previous observations that cardiac activity encodes complex information processing and their variations depending on sleep states during sleep (Koroma et al., 2024; Pelentritou et al., 2024; Whitehurst et al., 2020). They also confirm previous demonstrations obtained in DOC patients that cardiac responses to the auditory local-global paradigm inform about variations of cognitive processing across conscious states beyond cerebral findings (Raimondo et al., 2017). Studies investigating the cerebral processing of cardiac responses (*e.g.*, heart-evoked potential) may complement our study by offering a more integrated account of the brain-body correlates of auditory irregularity processing during sleep, as it has already been done in DOC patients (Candia-Rivera et al., 2023).

At the same time, our complementary methodology to (Raimondo et al., 2017) shows that the duration of PRE and POST periods influenced the cardiac effects reported in NREM and REM sleep. We interpret this finding as an effect of baseline variations of heart rate on cardiac responses to auditory stimuli. Despite the study of the interaction between baseline and evoked changes of cardiac activity is beyond the scope of the current study, determining the origin of this effect in the future might help to better control for the parameters shaping cardiac reactivity to environmental demands.

Finally, global deviance effects were also observed in cerebral activity during sleep when analyses included trials that were also presented in wakefulness before (Strauss et al., 2015). The possibility of such carry-over effects from wakefulness to sleep due to previous exposure of stimuli is undermined at the cardiac level because we found an absence of cardiac modulation to auditory irregularities in wakefulness. The effect of training may nevertheless

be investigated in future studies to gain insights on the role of automatized processes on cardiac responses to sensory information during sleep.

In conclusion, we report that cardiac responses to the auditory local-global paradigm reveal the processing of complex irregularities (*i.e.*, global deviance effects) during REM sleep, and basic irregularities (*i.e.*, local mismatch effects) in NREM sleep. Some of our findings diverge from our initial predictions based on the study of cerebral effects (Blume et al., 2022; Strauss et al., 2015, 2022), confirming previous demonstrations that cardiac signals encode information about cognitive processes that are partially independent from brain activity during sleep (Koroma et al., 2024; Whitehurst et al., 2016, 2022). Overall, our study provides novel evidence supporting the embodiment of cognitive functions and highlights the value of cardiac signals to gain insight on the correlates of complex information processing during sleep.

### **Competing interests**

The authors declare no competing interests.

### **Data and code availability**

Codes and dataframes used for analyses are in open access via [https://gitlab.uliege.be/Matthieu.Koroma/sleep\\_localglobal/-/tree/master/preprint](https://gitlab.uliege.be/Matthieu.Koroma/sleep_localglobal/-/tree/master/preprint)

### **Author contributions**

**Matthieu Koroma:** Conceptualization; investigation; writing – original draft; methodology; validation; visualization; writing – review and editing; project administration; formal analysis; software; data curation; resources; funding acquisition; supervision.

**Paradeisos Boulakis:** Methodology; validation; writing – review and editing; resources.

**Vaia Gialama:** Methodology; validation; formal analysis.

**Federico Raimondo:** Conceptualization; methodology; validation; writing – review and editing; resources.

**Christine Blume:** Methodology; validation; visualization; writing – review and editing; project administration; formal analysis; data curation; resources; supervision.

**Mélanie Strauss:** Conceptualization; Methodology; validation; visualization; writing – review and editing; project administration; formal analysis; data curation; resources; supervision; funding acquisition.

**Athena Demertzi:** Supervision; conceptualization; investigation; validation; visualization; writing – review and editing; formal analysis; project administration; resources; data curation; methodology; writing – original draft; funding acquisition.

### **Funding information**

H2020 European Research Council, Grant/Award Numbers: 667875, 757763; Fonds De La Recherche Scientifique - FNRS, Grant/Award Numbers: 40005128 (MK), 40016559 (PB), 40003373 (AD), 40010566 (MS); EU Horizon 2020 Research and Innovation Marie Skłodowska-Curie RISE program “NeuronsXnets”, Grant/Award Number: 101007926; European Cooperation in Science and Technology (COST Action) Program “NeuralArchCon”, Grant/Award Number: CA18106. CB was supported by a fellowship of the Austrian Science Fund (FWF; J-4243), a grant from the Research Fund for Junior Researchers of the University of Basel, an Ambizione grant from the Swiss National Science Foundation (SNF; PZ00P1\_201742), and funds from the Freiwillige Akademische Gesellschaft (FAG) and the Novartis Foundation for Biological-Medical Research.

### **References**

Andrillon, T., & Kouider, S. (2020). The vigilant sleeper: Neural mechanisms of sensory (de)coupling during sleep. *Current Opinion in Physiology*, 15, 47–59.  
<https://doi.org/10.1016/j.cophys.2019.12.002>



- Arnulf, I. (2011). The ‘scanning hypothesis’ of rapid eye movements during REM sleep: A review of the evidence. *Archives Italiennes de Biologie*, 149, Article 149.  
<https://doi.org/10.4449/aib.v149i4.1246>
- Azzalini, D., Rebollo, I., & Tallon-Baudry, C. (2019). Visceral Signals Shape Brain Dynamics and Cognition. *Trends in Cognitive Sciences*, 23(6), Article 6.  
<https://doi.org/10.1016/j.tics.2019.03.007>
- Bamiou, D.-E., Musiek, F. E., & Luxon, L. M. (2003). The insula (Island of Reil) and its role in auditory processing. *Brain Research Reviews*, 42(2), 143–154.  
[https://doi.org/10.1016/S0165-0173\(03\)00172-3](https://doi.org/10.1016/S0165-0173(03)00172-3)
- Battaglia, S., Nazzi, C., Lonsdorf, T. B., & Thayer, J. F. (2024). Neuropsychobiology of fear-induced bradycardia in humans: Progress and pitfalls. *Molecular Psychiatry*.  
<https://doi.org/10.1038/s41380-024-02600-x>
- Bayne, T., Seth, A. K., Massimini, M., Shepherd, J., Cleeremans, A., Fleming, S. M., Malach, R., Mattingley, J. B., Menon, D. K., Owen, A. M., Peters, M. A. K., Razi, A., & Mudrik, L. (2024). Tests for consciousness in humans and beyond. *Trends in Cognitive Sciences*, 28(5), 454–466. <https://doi.org/10.1016/j.tics.2024.01.010>
- Bekinschtein, T. A., Dehaene, S., Rohaut, B., Tadel, F., Cohen, L., & Naccache, L. (2009). Neural signature of the conscious processing of auditory regularities. *Proceedings of the National Academy of Sciences*, 106(5), 1672–1677.  
<https://doi.org/10.1073/pnas.0809667106>
- Benarroch, E. E. (2018). Brainstem integration of arousal, sleep, cardiovascular, and respiratory control. *Neurology*, 91(21), 958–966.  
<https://doi.org/10.1212/WNL.0000000000006537>

- Benjamini, Y., & Yekutieli, D. (2001). The control of the false discovery rate in multiple testing under dependency. *The Annals of Statistics*, 29(4).  
<https://doi.org/10.1214/aos/1013699998>
- Blume, C., Niedernhuber, M., Spitschan, M., Slawik, H. C., Meyer, M. P., Bekinschtein, T. A., & Cajochen, C. (2022). Melatonin suppression does not automatically alter sleepiness, vigilance, sensory processing, or sleep. *Sleep*, 45(11), zsac199.  
<https://doi.org/10.1093/sleep/zsac199>
- Blume, C., & Schabus, M. (2019). *Sentinel or rather standby? Regardless of terminology, information processing continues during sleep*. <https://doi.org/10.31219/osf.io/bq8hr>
- Candia-Rivera, D., Raimondo, F., Pérez, P., Naccache, L., Tallon-Baudry, C., & Sitt, J. D. (2023). Conscious processing of global and local auditory irregularities causes differentiated heartbeat-evoked responses. *eLife*, 12, e75352.  
<https://doi.org/10.7554/eLife.75352>
- Chouchou, F., & Deseilles, M. (2014). Heart rate variability: A tool to explore the sleeping brain? *Frontiers in Neuroscience*, 8. <https://doi.org/10.3389/fnins.2014.00402>
- Cirelli, C., & Tononi, G. (2008). Is Sleep Essential? *PLoS Biology*, 6(8), Article 8.  
<https://doi.org/10.1371/journal.pbio.0060216>
- Coenen, A. (2024). Sensory gating and gaining in sleep: The balance between the protection of sleep and the safeness of life (a review). *Journal of Sleep Research*, 33(5), e14152.  
<https://doi.org/10.1111/jsr.14152>
- de Zambotti, M., Trinder, J., Silvani, A., Colrain, I. M., & Baker, F. C. (2018). Dynamic coupling between the central and autonomic nervous systems during sleep: A review. *Neuroscience & Biobehavioral Reviews*, 90, 84–103.  
<https://doi.org/10.1016/j.neubiorev.2018.03.027>

- Ermis, U., Krakow, K., & Voss, U. (2010). Arousal thresholds during human tonic and phasic REM sleep: Arousal threshold in tonic and phasic REM. *Journal of Sleep Research*, 19(3), Article 3. <https://doi.org/10.1111/j.1365-2869.2010.00831.x>
- Griffiths, T. D., Uppenkamp, S., Johnsrude, I., Josephs, O., & Patterson, R. D. (2001). Encoding of the temporal regularity of sound in the human brainstem. *Nature Neuroscience*, 4(6), 633–637. <https://doi.org/10.1038/88459>
- Hennevin, E., Huetz, C., & Edeline, J.-M. (2007). Neural representations during sleep: From sensory processing to memory traces. *Neurobiology of Learning and Memory*, 87(3), Article 3. <https://doi.org/10.1016/j.nlm.2006.10.006>
- Iber, C., Ancoli-Israel, S., Chesson, A. L., & Quan, S. F. (2007). *The AASM manual for the scoring of sleep and associated events: Rules, terminology and technical specifications (Vol. 1)*. Westchester, IL: American Academy of Sleep Medicine.
- Kass, R. E., & Raftery, A. E. (1995). Bayes Factors. *Journal of the American Statistical Association*, 90(430), Article 430. <https://doi.org/10.1080/01621459.1995.10476572>
- Koroma, M., Beck, J., Schmidt, C., Rasch, B., & Demertzi, A. (2024). Probing the embodiment of sleep functions: Insights from cardiac responses to word-induced relaxation during sleep. *Journal of Sleep Research*, e14160. <https://doi.org/10.1111/jsr.14160>
- Koroma, M., Lacaux, C., Andrillon, T., Legendre, G., Léger, D., & Kouider, S. (2020). Sleepers Selectively Suppress Informative Inputs during Rapid Eye Movements. *Current Biology*, 30(12), Article 12. <https://doi.org/10.1016/j.cub.2020.04.047>
- Lacaux, C., Strauss, M., Bekinschtein, T. A., & Oudiette, D. (2024). Embracing sleep-onset complexity. *Trends in Neurosciences*, 47(4), 273–288. <https://doi.org/10.1016/j.tins.2024.02.002>

Laureys, S. (2005). The neural correlate of (un)awareness: Lessons from the vegetative state.

*Trends in Cognitive Sciences*, 9(12), Article 12.

<https://doi.org/10.1016/j.tics.2005.10.010>

Legendre, G., Andrillon, T., Koroma, M., & Kouider, S. (2019). Sleepers track informative speech in a multitalker environment. *Nature Human Behaviour*, 3(3), Article 3.

<https://doi.org/10.1038/s41562-018-0502-5>

Makov, S., Sharon, O., Ding, N., Ben-Shachar, M., Nir, Y., & Zion Golumbic, E. (2017).

Sleep Disrupts High-Level Speech Parsing Despite Significant Basic Auditory

Processing. *The Journal of Neuroscience: The Official Journal of the Society for*

*Neuroscience*, 37(32), Article 32. <https://doi.org/10.1523/JNEUROSCI.0168-17.2017>

Makowski, D., Pham, T., Lau, Z. J., Brammer, J. C., Lespinasse, F., Pham, H., Schölzel, C.,

& Chen, S. H. A. (2021). NeuroKit2: A Python toolbox for neurophysiological signal processing. *Behavior Research Methods*, 53(4), 1689–1696.

<https://doi.org/10.3758/s13428-020-01516-y>

Muzur, A., Pace-Schott, E. F., & Hobson, J. A. (2002). The prefrontal cortex in sleep. *Trends in Cognitive Sciences*, 6(11), 475–481. [https://doi.org/10.1016/S1364-](https://doi.org/10.1016/S1364-6613(02)01992-7)

[6613\(02\)01992-7](https://doi.org/10.1016/S1364-6613(02)01992-7)

Ogilvie, R. D. (2001). The process of falling asleep. *Sleep Medicine Reviews*, 5(3), 247–270.

<https://doi.org/10.1053/smr.2001.0145>

Oppenheimer, S., & Cechetto, D. (2016). The Insular Cortex and the Regulation of Cardiac

Function. In Y. S. Prakash (Ed.), *Comprehensive Physiology* (1st ed., pp. 1081–1133).

Wiley. <https://doi.org/10.1002/cphy.c140076>

Peigneux, P., Laureys, S., Delbeuck, X., & Maquet, P. (2001). Sleeping brain, learning brain.

The role of sleep for memory systems. *Neuroreport*, 12(18), Article 18.

<https://doi.org/10.1097/00001756-200112210-00001>

- Pelentritou, A., Pfeiffer, C., Schwartz, S., & De Lucia, M. (2024). Cardio-audio synchronization elicits neural and cardiac surprise responses in human wakefulness and sleep. *Communications Biology*, 7(1), 226. <https://doi.org/10.1038/s42003-024-05895-2>
- Perrin, F. (1999). A differential brain response to the subject's own name persists during sleep. *Clinical Neurophysiology*, 110(12), Article 12. [https://doi.org/10.1016/S1388-2457\(99\)00177-7](https://doi.org/10.1016/S1388-2457(99)00177-7)
- Postuma, R. B., Lanfranchi, P. A., Blais, H., Gagnon, J., & Montplaisir, J. Y. (2010). Cardiac autonomic dysfunction in idiopathic REM sleep behavior disorder. *Movement Disorders*, 25(14), 2304–2310. <https://doi.org/10.1002/mds.23347>
- Raimondo, F., Rohaut, B., Demertzi, A., Valente, M., Engemann, D. A., Salti, M., Fernandez Slezak, D., Naccache, L., & Sitt, J. D. (2017). Brain-heart interactions reveal consciousness in noncommunicating patients: Brain-Heart Interactions. *Annals of Neurology*, 82(4), Article 4. <https://doi.org/10.1002/ana.25045>
- Rechtschaffen, A., Hauri, P., & Zeitlin, M. (1966). Auditory Awakening Thresholds in Rem and Nrem Sleep Stages. *Perceptual and Motor Skills*, 22(3), Article 3. <https://doi.org/10.2466/pms.1966.22.3.927>
- Sallinen, M., Kaartinen, J., & Lyytinen, H. (1996). Processing of auditory stimuli during tonic and phasic periods of REM sleep as revealed by event-related brain potentials. *Journal of Sleep Research*, 5(4), Article 4. <https://doi.org/10.1111/j.1365-2869.1996.00220.x>
- Simor, P., van der Wijk, G., Nobili, L., & Peigneux, P. (2020). The microstructure of REM sleep: Why phasic and tonic? *Sleep Medicine Reviews*, 52, 101305. <https://doi.org/10.1016/j.smr.2020.101305>

- Skora, L. I., Livermore, J. J. A., & Roelofs, K. (2022). The functional role of cardiac activity in perception and action. *Neuroscience & Biobehavioral Reviews*, 137, 104655.  
<https://doi.org/10.1016/j.neubiorev.2022.104655>
- Spreng, L. F., Johnson, L. C., & Lubin, A. (1968). AUTONOMIC CORRELATES OF EYE MOVEMENT BURSTS DURING STAGE REM SLEEP. *Psychophysiology*, 4(3), Article 3. <https://doi.org/10.1111/j.1469-8986.1968.tb02773.x>
- Strauss, M., Sitt, J. D., King, J.-R., Elbaz, M., Azizi, L., Buiatti, M., Naccache, L., van Wassenhove, V., & Dehaene, S. (2015). Disruption of hierarchical predictive coding during sleep. *Proceedings of the National Academy of Sciences*, 112(11), Article 11.  
<https://doi.org/10.1073/pnas.1501026112>
- Strauss, M., Sitt, J. D., Naccache, L., & Raimondo, F. (2022). Predicting the loss of responsiveness when falling asleep in humans. *NeuroImage*, 251, 119003.  
<https://doi.org/10.1016/j.neuroimage.2022.119003>
- Tononi, G., Boly, M., & Cirelli, C. (2024). Consciousness and sleep. *Neuron*, 112(10), 1568–1594. <https://doi.org/10.1016/j.neuron.2024.04.011>
- Tononi, G., & Massimini, M. (2008). *Why Does Consciousness Fade in Early Sleep ? Annals of the New York Academy of Sciences*, 1129(1), Article 1.  
<https://doi.org/10.1196/annals.1417.024>
- Vigo, D. E., Dominguez, J., Guinjoan, S. M., Scaramal, M., Ruffa, E., Solernó, J., Siri, L. N., & Cardinali, D. P. (2010). Nonlinear analysis of heart rate variability within independent frequency components during the sleep–wake cycle. *Autonomic Neuroscience*, 154(1–2), 84–88. <https://doi.org/10.1016/j.autneu.2009.10.007>
- Viola, A. U., Tobaldini, E., Chellappa, S. L., Casali, K. R., Porta, A., & Montano, N. (2011). Short-Term Complexity of Cardiac Autonomic Control during Sleep: REM as a

Potential Risk Factor for Cardiovascular System in Aging. *PLoS ONE*, 6(4), e19002.

<https://doi.org/10.1371/journal.pone.0019002>

Wehrle, R., Kaufmann, C., Wetter, T. C., Holsboer, F., Auer, D. P., Pollmächer, T., &

Czisch, M. (2007). Functional microstates within human REM sleep: First evidence from fMRI of a thalamocortical network specific for phasic REM periods. *The European Journal of Neuroscience*, 25(3), Article 3. <https://doi.org/10.1111/j.1460-9568.2007.05314.x>

Whitehurst, L. N., Cellini, N., McDevitt, E. A., Duggan, K. A., & Mednick, S. C. (2016).

Autonomic activity during sleep predicts memory consolidation in humans.

*Proceedings of the National Academy of Sciences*, 113(26), Article 26.

<https://doi.org/10.1073/pnas.1518202113>

Whitehurst, L. N., Chen, P.-C., Naji, M., & Mednick, S. C. (2020). New directions in sleep

and memory research: The role of autonomic activity. *Current Opinion in Behavioral Sciences*, 33, 17–24. <https://doi.org/10.1016/j.cobeha.2019.11.001>

Whitehurst, L. N., Subramoniam, A., Krystal, A., & Prather, A. A. (2022). Links between the

brain and body during sleep: Implications for memory processing. *Trends in Neurosciences*, 45(3), 212–223. <https://doi.org/10.1016/j.tins.2021.12.007>

Wong, S. W., Massé, N., Kimmerly, D. S., Menon, R. S., & Shoemaker, J. K. (2007). Ventral

medial prefrontal cortex and cardiovagal control in conscious humans. *NeuroImage*, 35(2), 698–708. <https://doi.org/10.1016/j.neuroimage.2006.12.027>

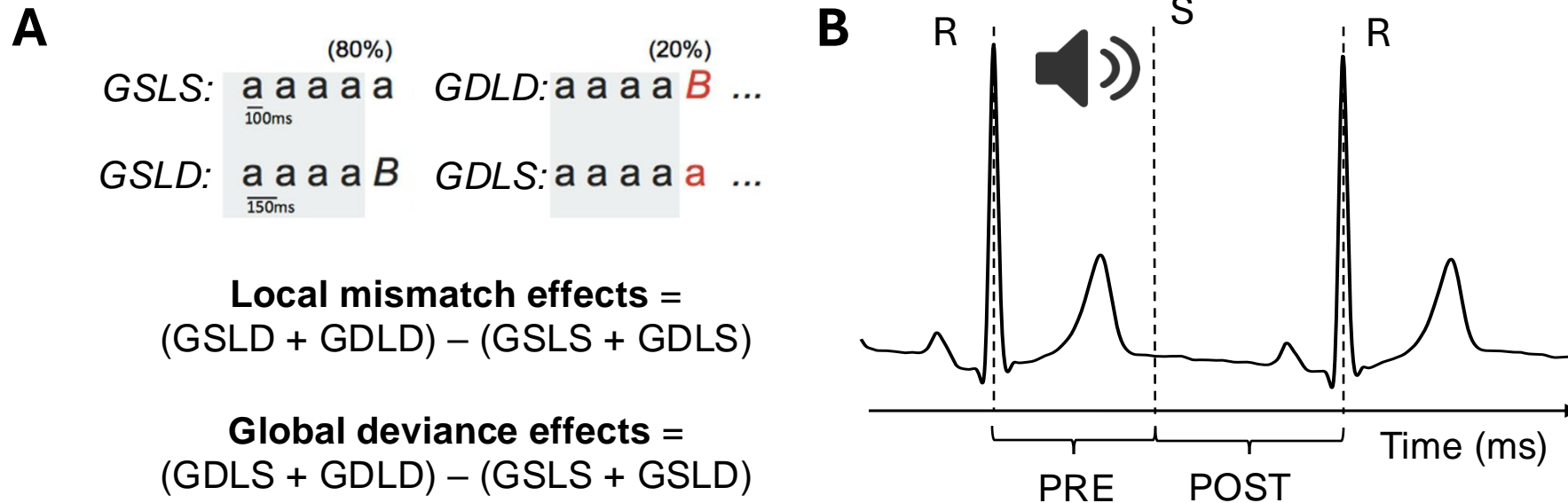


Figure 1. **Analysis of the local-global paradigm played during sleep across two datasets.** **(A)** A trial was composed of a sequence of 5 tones and belonged to one of the 4 following categories: global standard and local standard (GSLS, top left), global deviant and local deviant (GDLD, top right), global standard and local deviant (GSLD, bottom left) or global deviant and local standard (GDLS, bottom right). Local mismatch effects were defined as the difference from local deviants with local standards and global deviance effects were defined as the difference between global deviants and global standards. Adapted from Strauss et al., 2015; 2022 **(B)** Heartbeats were extracted from ECG and the duration between onset of the 5th sound and the preceding (PRE) and following heartbeat (POST) was computed for each trial.



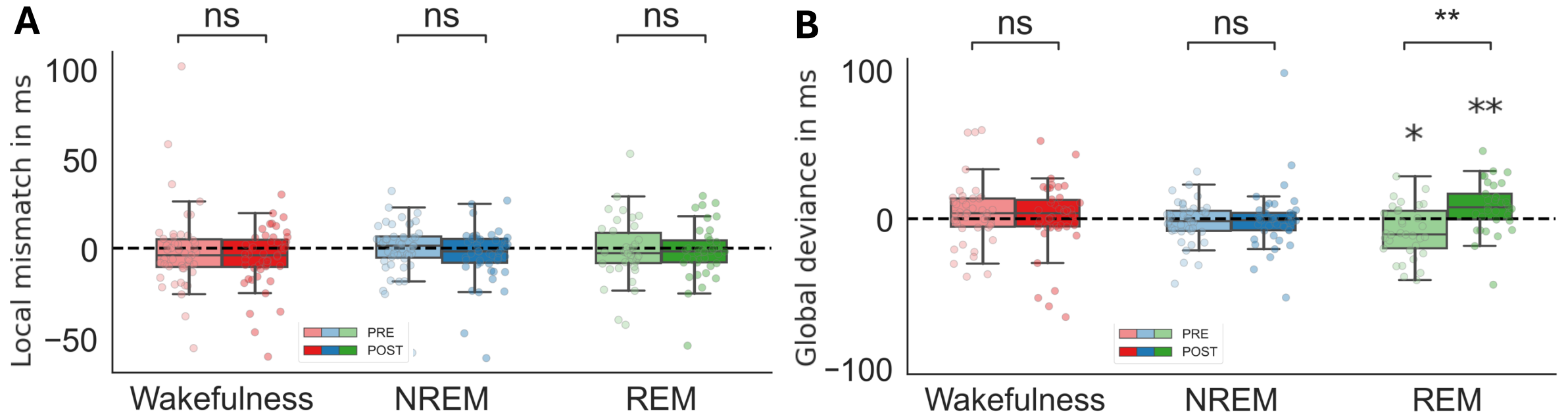


Figure 2. **Cardiac activity decelerates after global deviants in REM sleep.** Local mismatch (A) and global deviance (B) effects of cardiac responses were computed for Wakefulness, NREM and REM separately for the PRE and POST periods with respect to the fifth sound of the local-global paradigm (contained between 20 and 600ms). Boxplots represent median, 1<sup>st</sup> and 4<sup>th</sup> quartiles and deciles of effects across subjects are represented by boxplots in each sleep state. Datapoints represent individual subjects. Statistical significance of post-hoc tests, ns: not significant, \*:  $p < 0.05$ , \*\*:  $p < 0.01$ .

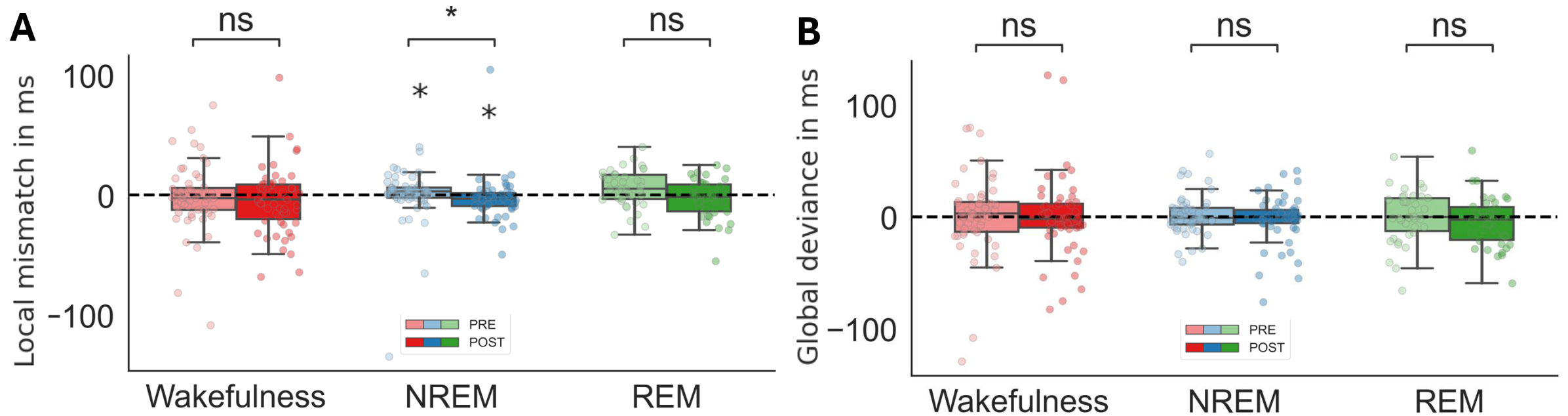


Figure 3. **Cardiac activity accelerates after local deviants during NREM sleep.** Local mismatch (**A**) and global deviance (**B**) effects were computed for Wakefulness, NREM and REM separately for PRE and POST periods (contained between 20 and 900ms, following a grid-search analysis). Boxplots represent median, first and fourth quartiles and whiskers deciles for each condition. Datapoints represent individual subjects. Statistical significance for post-hoc test, ns: not significant, \*:  $p < 0.05$

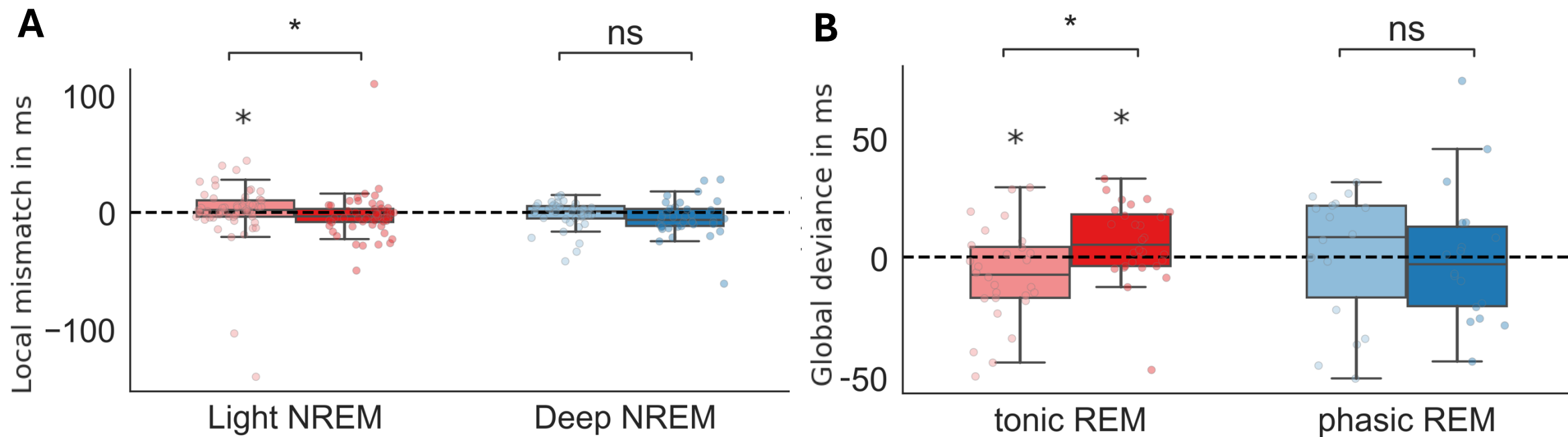
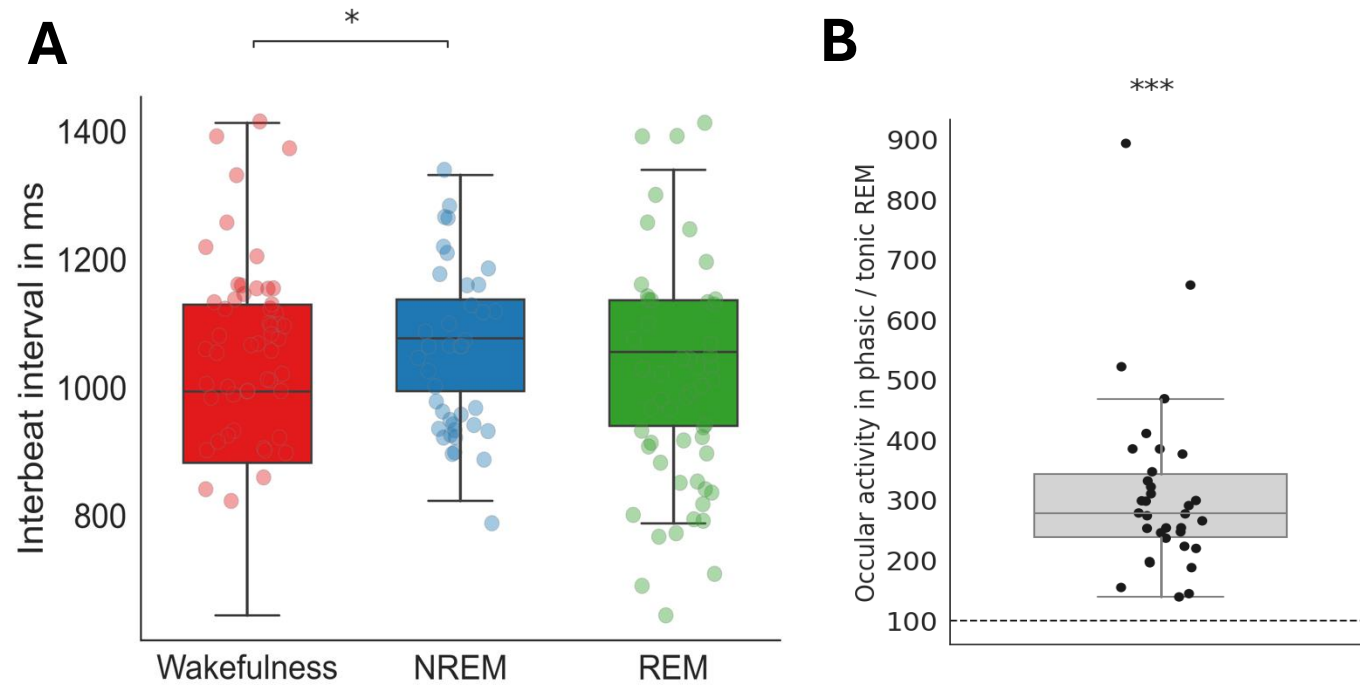


Figure 4. **Cardiac activity is modulated in light NREM and tonic REM sleep.** Local mismatch effects were computed for PRE and POST periods contained between 20 and 900ms in light and deep NREM (A) and between 20 and 600ms global deviance effects in tonic and phasic REM (B). Boxplots represent median, first and fourth quartiles and whiskers deciles for each condition. Datapoints represent individual subjects. Statistical significance for post-hoc tests, ns: not significant, \*:  $p < 0.05$



**Figure S1. Cardiac and ocular signals are modulated across sleep stages.** (A) Interbeat interval were computed by extracting R-peaks from electrocardiographic signals and averaging over sleep scoring windows of the same stage for each subject. (B) Ocular activity was defined as the standard deviation of electrooculographic signals around trial onset (-4s to 4s). Statistical significance for post-hoc tests, \*:  $p < 0.05$ , \*\*\*:  $p < 0.001$

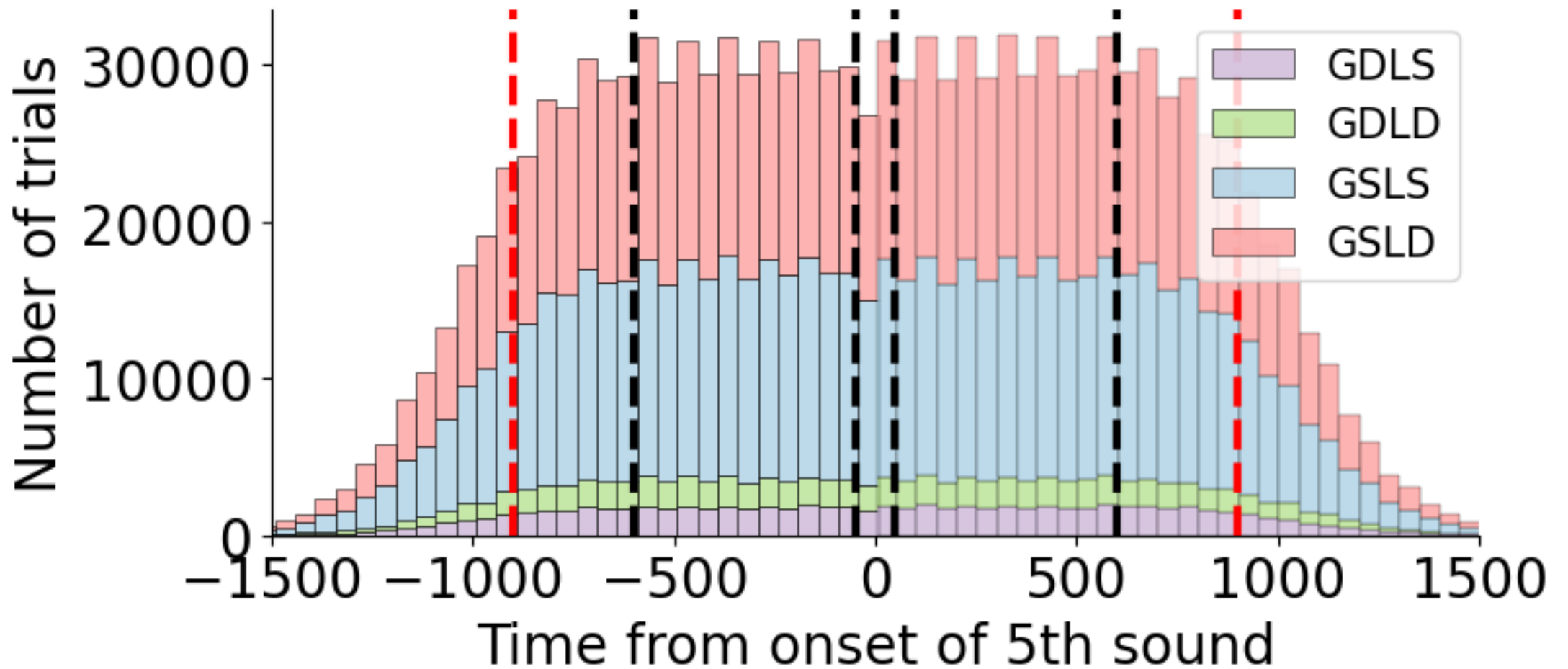


Figure S2. **PRE and POST periods were defined based on heartbeats around 5th sound onset.** PRE periods were defined based on heartbeats before the onset of the 5th sound (negative values) and POST periods based on heartbeats after the onset of the 5th sound (positive values). GDLS: Global Deviant Local Standard, GDLD: Global Deviant Local Standard, GSLS: Global Standard Local Standard, GSLD: Global Standard Local Deviant. Black dotted lines: 20 and 600ms defining the bounds of PRE and POST periods included for confirmatory analyses. Red dotted lines: 900ms defining the upper bound of PRE and POST periods included for exploratory analyses.

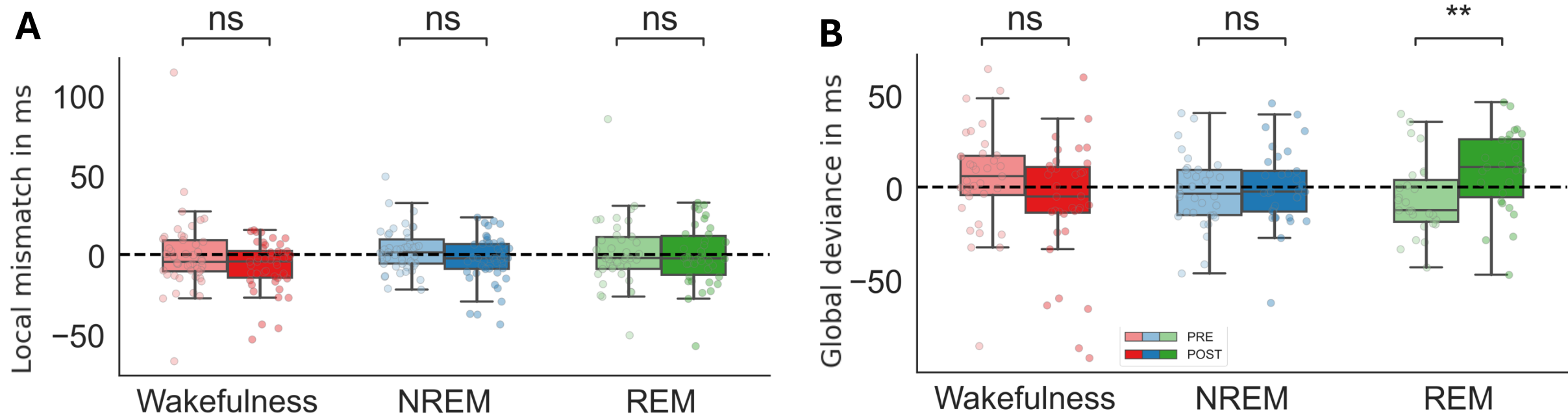


Figure S3. **Cardiac decelerates after “true global” deviants during REM sleep.** “True local” mismatch (**A**) and “true global” deviance (**B**) effects were computed for Wakefulness, NREM and REM separately for PRE and POST periods contained between 20 and 600ms following Raimondo et al., 2017. Boxplots represent median, first and fourth quartiles and whiskers deciles for each condition. Datapoints represent individual subjects. Statistical significance for post-hoc test, ns: not significant, \*:  $p < 0.05$ , \*\*:  $p < 0.01$

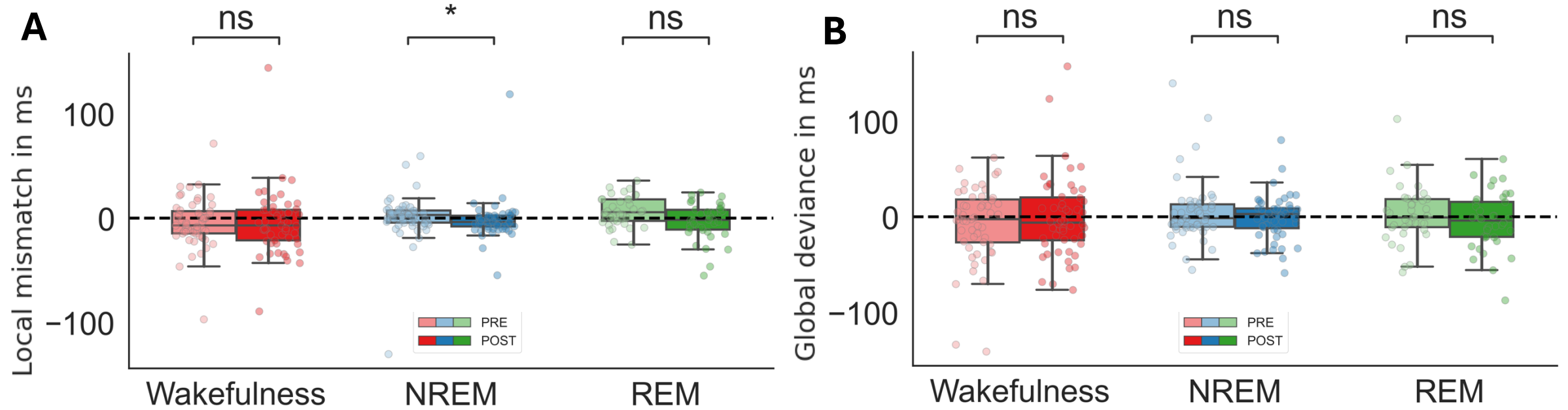


Figure S4. **Cardiac activity accelerates after “true local” deviants during NREM sleep.** “True local” mismatch (**A**) and “true global” deviance (**B**) effects were computed for Wakefulness, NREM and REM separately for PRE and POST periods contained between 20 and 900ms following the grid-search analysis. Boxplots represent median, first and fourth quartiles and whiskers deciles for each condition. Datapoints represent individual subjects. Statistical significance for post-hoc test, ns: not significant, \*:  $p < 0.05$

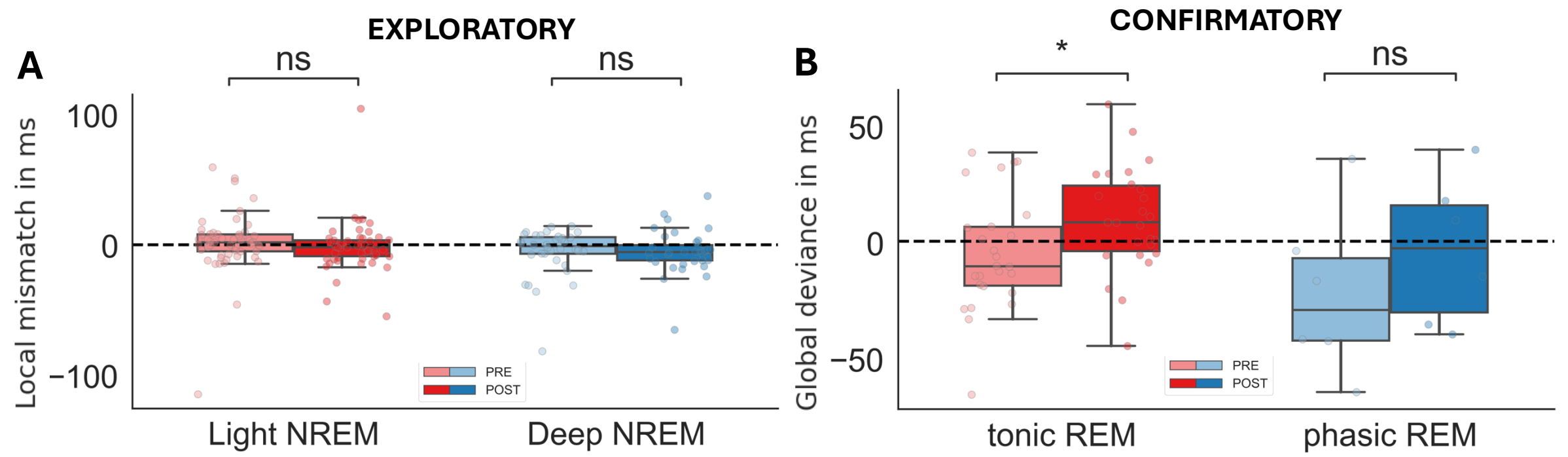


Figure S5. **Cardiac responses decelerate after “true global” deviants in tonic REM.** True local mismatch effects were computed for PRE and POST periods contained between 20 and 900ms in light and deep NREM (**A**) and true global deviance between 20 and 600ms effects in tonic and phasic REM (**B**). Boxplots represent median, first and fourth quartiles and whiskers deciles for each condition. Datapoints represent individual subjects. Statistical significance for post-hoc test, ns: not significant, \*:  $p < 0.05$



**Table S1. Grid-search analysis approach identifies a local mismatch effect during sleep when including PRE and POST periods from 20 to 900ms.** The median and 95% confidence interval (bootstrap, n=2000) of the POST-PRE and the post-hoc Wilcoxon test POST vs. PRE corrected for multiple comparisons were computed for the local mismatch and global deviance effects in wakefulness and sleep (NREM2, NREM3 and REM grouped together) on PRE and POST periods ranging between 20ms and 600 until 1200ms with 100ms step interval. Statistical significance, \*: p<0.05

Effect	State	600ms	700ms	800ms	900ms	1000ms	1100ms	1200ms
Local mismatch	Wake	-2.6± [-8.6, 4.9]	-6.3± [-14.1, -1.8]	-3.2± [-8.5, 7.2]	0.01± [-12.4, 8.4]	-7.3± [-20.3, 0.3]	-3.7± [-16.6, -0.5]	-2.3± [-20.7, -2.5]
	Sleep	-2.2± [-5.0, -1.1]	-3.0± [-6.4, -0.8]	-3.4± [-6.0, -0.2]	<b>-5.4± [-10.2, -3.0]*</b>	-3.3± [-9.1, 0.9]	-4.3± [-9.8, 0.5]	-4.4± [-9.2, 2.6]
Global deviance	Wake	0.9± [-10.3, 9.1]	-9.3± [-16.1, 4.7]	-2.5± [-12.3, 9.6]	-7.4± [-12.9, 7.9]	-0.1± [-15.4, 17.9]	1.7± [-13.4, 18.8]	6.5± [-8.6, 19.4]
	Sleep	3.5± [-1.1, 15.8]	1.2± [-6.4, 6.1]	0.8± [-8.8, 7.0]	-2.7± [-7.7, 2.3]	-2.8± [-9.1, 7.4]	-5.6± [-8.3, 3.4]	-4.7± [-9.0, 3.6]